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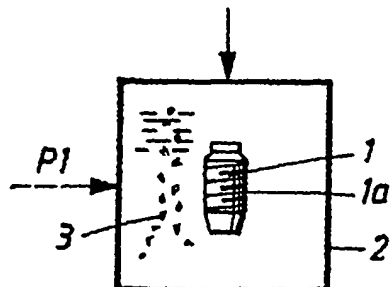
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(54) Title: IMPLANT FOR APPLICATION IN BONE, METHOD FOR PRODUCING SUCH AN IMPLANT, AND USE OF SUCH AN IMPLANT



(57) Abstract: An implant (1) for application in bone (8), for example the jaw bone, primarily of the human body, comprises a unit (1) which can be applied in the bone in question and which is made of biocompatible material, preferably titanium (18). On its surface parts cooperating with the bone, the unit is provided with a coating (or coatings) of an agent (substance) TS, which initiates and/or stimulates bone growth. The coating (or coatings) comprises (comprise) calcium phosphate compounds CaP and the said stimulating agent TS.

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## TITLE

Implant for application in bone, method for producing such an implant, and use of such an implant

## 5 TECHNICAL FIELD

The present invention relates to an implant for application in bone, for example the jaw bone, primarily of the human body. The implant comprises a unit which can be applied in the bone in question and  
10 which is made of biocompatible material, preferably titanium. At least on its surface parts cooperating with the bone, the unit is provided with a coating (or coatings) as will be described below. The invention also relates to a method for producing such an implant  
15 and to the use of such an implant.

## PRIOR ART

It is already known to coat implants with films or layers on those parts which are directed towards the  
20 bone in question, for example the jaw bone. The coating is intended to initiate and stimulate bone growth where the implant has been implanted or screwed into place. It is known to use hydroxyapatite or HA in the coating. The said HA can be produced by various methods, of  
25 which one advantageous method has been found to be a method called RF sputtering, with subsequent heat treatment. It is known to use calcium phosphate compounds to achieve different release times during which the agent migrates from the layer to the  
30 surrounding bone material/jaw bone material, using different degrees of crystallization. The higher the degree of crystallization, the longer the release time, and vice versa.

Reference may be made to WO 98/48862 from the  
35 same Applicant as in the present case. The said publication gives examples of methods for applying layers of this type, and layer structures which are applicable in the present invention.

Reference may be made in purely general terms to WO 88/08460 and WO 94/25637. Reference is also made to the publications "Biomaterials, Volume 17, No. 4, 1996, K. Van Dijk et al., Influence of annealing  
5 temperature on RF magnetron sputtered calcium phosphat coatings, page 405 to page 410" and "Journal of Biomedical Materials Research, Volume 28, 1994, J. G. C. Wolke et al., Study of the surface characteristics of magnetron-sputter calcium phosphate coatings, page  
10 1477 to page 1484" and "Phosphorus Research Bulletin, Volume 6, 1996, Kimihiro Yamashita et al., Bone-Like Apatite Coating of Alumina and Zirconia by RF-Magnetron Sputtering, page 123 to page 126".

In connection with titanium implants, it is  
15 also known to arrange thick, porous titanium oxide layers which are used as depots for, inter alia, bone-growth-stimulating agents/substances (TS). In this connection, reference may be made to Swedish Patent Application No. 99 01971-3 filed on the same day  
20 and by the same Applicant, and which starts from the known arrangements according to the publications "Journal of Biomedical Materials Research, by Dann et al., Gentamicin sulfate attachment and release from anodized Ti-6Al-4V orthopedic materials, Vol. 27, 895-  
25 900 (1993)" and "Journal of Biomedical Materials Research, by Hitoshi Ishizawa and Makoto Ogino, Formation and characterization of anodic titanium oxide films containing Ca and P, Vol. 29, 65-72 (1995)".

Reference is made in purely general terms to  
30 US Patents 4,330,891 and 5,354,390.

#### TECHNICAL PROBLEM

At the present time, considerable efforts are being made to further develop and refine the implants,  
35 methods and uses in question here. Particularly in the case of a bone/jaw bone in which it is not entirely certain that the implant will incorporate in the bone, it is preferable to be able to call upon and use all the possibilities at present available in the areas in

question, inter alia the dental area. The invention aims to solve this problem, among others.

There is a need to be able to control more exactly the release times for the transfer of the agents/substances from the implant layer to the surrounding bone tissue. Thus, for example, it may be necessary to achieve a better controlled release function during a defined or optimum time for the agents or the substances. The invention solves this problem too.

In certain cases, it is preferable for the implant surface cooperating with the bone structure to still have the prescribed degree of fineness even after the coating or coatings have been applied, in order, in certain implant cases, to be able to maintain relatively small tightening forces/screwing forces, for example for a tooth implant in a hole in the jaw bone. The invention solves this problem too.

Using a relatively coarse porosity can increase the tightening force considerably, which may be advantageous in certain cases but which should be avoided in other cases, especially in connection with hard bones. It may be noted here that improved healing processes in soft bones are needed. The invention solves this problem too.

It is also preferable to be able to use proven methods for producing the relevant type of implant despite the fact that the implant has better properties from the medical point of view. The invention solves this problem too.

It is often necessary to be able to accelerate the healing time for an implant. This can be controlled by suitable choice of coating or coatings. There are also problems in being able to correctly balance the initial bone growth stimulation and the long-term maintenance of the established bone growth. If bone growth is too rapid, this may give rise to bone fractures and other complications in bone growth. A long-term stimulation or the maintenance of bone growth

are important for an implant which is to function for a long time or for many years without the implant needing to be changed. The invention solves this problem too.

In accordance with the invention, a bone-  
5 growth-stimulating substance or agent, here called TS, is to be used. Examples which may be mentioned are those substances belonging to the superfamily TGF- $\beta$ , for example BMP (Bone Morphogenetic Proteins). There may be problems in preventing the said rapid release of  
10 the TS in question. It is also preferable to be able to obtain a functionally reliable support for TS upon application to an implant surface which from the outset is amorphous or heat-treated and partially crystalline. The invention solves this problem too.

15 There is also a need to have access to a wider range and choice of implant types which will be able to satisfy different applications on the market, cf. implants for soft bone and hard bone, etc. The invention solves this problem too.

20

#### SOLUTION

The feature which can principally be regarded as characterizing an implant according to the invention  
25 is that the coating or coatings comprise a CaP coating with added TS. (CaP = calcium phosphate, and TS = growth-stimulating substance).

In embodiments of the inventive concept, the time for the said agent in the said coating or coatings  
30 to be released to the surrounding bone or tissue is chosen by setting the release time for CaP and the release time for TS in relation to each other. The release time for CaP is chosen with the aid of the degree of crystallization in CaP. The total release  
35 time can be chosen within the range from a few days to several months. In one embodiment, TS is applied on top of CaP. In one embodiment, the CaP coating can have a thickness in the range of between a few angstroms and 10  $\mu\text{m}$ . In another illustrative embodiment, values in

the range of between 0.1  $\mu\text{m}$  and 20  $\mu\text{m}$  can be used. All those areas of the said unit which cooperate with or are facing the bone material are preferably coated with the coating or layer in question. Each TS layer can  
5 have a thickness in the range of between a few angstroms and 1  $\mu\text{m}$ .

In one embodiment, the coating or coatings comprise one or more layers of calcium phosphate compounds and one or more layers of bone-growth-  
10 stimulating substance. Agents of the release-retarding type, for example hyaluronic acid, can be interleaved with the said layers. In a further illustrative embodiment, one or more layers of CaP can have a high degree of crystallization, for example 75-100%, which  
15 means that the layer or layers have the principal role of functioning as supports for the layer or layers of TS and possibly the release-retarding agent or agents. In a further embodiment, one or more layers of CaP can have a low or medium-high degree of crystallization,  
20 for example a degree of crystallization of between slightly over 0% and 75%, which means that the layer or layers exert a support function for TS, and possibly layers of release-retarding agents are included in the bone-growth-stimulating function. The layer or layers  
25 of CaP are preferably applied nearest to or on the actual surfaces of the implant. One or more layers of TS can be applied in turn on the last-mentioned layer or on the outer of the last-mentioned layers. In the case with two or more layers of TS, layers or agents  
30 with a release-retarding function are arranged between or outside the TS layers. At least the layer or layers of TS with possible release-retarding agent can be released with components occurring naturally in the bone and/or the tissue. The said layers and possible  
35 release-retarding agents are arranged or chosen to generate bone formation around the implant, without risk of excessively rapid bone build-up and bone fracture tendencies or other complications in the bone. The said layers and possible release-retarding agents

can also be arranged to effect an initially optimum bone structure around the implant in combination with long-term (over several months) bone growth or bone-growth-stimulating function. In one embodiment, one or  
5 more CaP layers consist of hydroxyapatite or HA, and one or more layers of the bone-growth-stimulating substance consist of BMP. The release-retarding agent can have a thickness of about 0.1 - 1.0  $\mu\text{m}$ .

A method according to the invention can  
10 principally be regarded as being characterized by the fact that the said parts of the unit or the whole unit are/is coated with CaP which can be given a defined degree of crystallization by heat treatment, and TS.

CaP is preferably first applied and heat-  
15 treated, after which TS is added, for example by means of the unit, or its relevant parts to be provided with coating, being dipped in a bath of TS. Alternatively, TS can be dropped or painted onto the implant.

In a preferred embodiment, in the case where  
20 there are several TS layers, the first layer is obtained by immersing in or dropping on or painting on a TS solution with a chosen concentration. The second layer is obtained, after drying of the first layer, by dropping on or painting on of a TS solution with the  
25 chosen concentration or a second concentration which differs from the first concentration. A possible third layer is obtained, after drying of the second layer, by dropping on or painting on a TS solution with a concentration which is the same as or differs from the  
30 previously mentioned concentrations, etc. Release-retarding agents can be applied, for example by painting, on the respective dried layer. The CaP layer can be applied by so-called sputtering of CaP substance onto one or more implant surfaces which can be  
35 amorphous or heat-treated and thus crystalline. The CaP layer can be made with depressions which facilitate the holding of the outlying TS layer. Such an implant with layers of CaP and outer-lying TS layers is applied in a threaded hole in the jaw bone or equivalent in one

proposed embodiment. Application methods for TS other than those mentioned can be used, for example spraying. A layer with a very high concentration of BMP can also be used.

- 5           A use, according to the invention, of the implant of the type in question is characterized essentially in that CaP and TS are used in the said coating or coatings.

10                           ADVANTAGES

- The invention makes two-fold use of substances which are known per se, which have bone-growth-stimulating properties and which at least in part are already naturally present in the human body. The use of porous oxide layers in the actual implant material as a depot for growth-stimulating substance or substances has forced the skilled person away from proposals in accordance with the present invention, principally on account of the fact that in certain cases the tightening force for the implant in bone provided with holes has had to be increased. This is not in itself a disadvantage if the total range which is to satisfy different requirements on the market is considered. The release times can, according to the invention, be chosen with great precision. The TS applied on top of the CaP coating often has greater volatility than CaP. In this way, TS can provide the surrounding jaw bone with a bone-growth-stimulating function in an initial stage, which function is gradually overtaken by the CaP coating. In one illustrative embodiment, one and the same implant serves two tissue sites located at a distance from each other.

DESCRIPTION OF THE FIGURES

- 35           A presently proposed embodiment of an arrangement, method and use according to the invention will be described below with reference to the attached drawings, in which:



Figures 1 - 4 show different stages in coating an implant with CaP layers and TS layers,

Figure 5 shows, in a vertical view and in cross section, and enlarged in relation to Figures 1 - 4, an actual implant applied in a hole made in the jaw bone,

Figure 6 shows, in graph form, release functions for the CaP and TS combination in the jaw bone,

Figure 7 shows, in a vertical view and in cross section, and enlarged in relation to Figure 5, the CaP and TS layers applied to the surface part in question,

Figure 8 shows, in a vertical view and in cross section, and enlarged in relation to Figure 7, the incorporation of the TS with the crystal structure of the CaP layer,

Figures 9 and 9a show, in vertical views and in cross sections, and on an enlarged scale, the CaP and TS layers applied as multi-layers,

Figures 10 to 12 show, in vertical sections and on an enlarged scale, the release function for multi-layers in tissue or jaw bone in the human body,

Figure 13 shows, in vertical section and on an enlarged scale, an alternative embodiment with multi-layers, and

Figures 14 and 15 show, in vertical sections, different examples of bone formation in tissue or bone.

#### DETAILED EMBODIMENT

A unit in the form of an implant is shown by 1 in Figure 1. The surface parts 1a of the implant are to be completely or partially provided with a film-like or layered coating (or coatings). A first coating is applied in a known manner in a chamber 2, the coating being applied by so-called RF sputtering. Reference is made here to the publication WO 98/48862 mentioned in the introduction. In the chamber 2, one or more calcium phosphate compounds 3 are applied to the surface or surface parts of the unit.

After application of the actual coating, the unit 1 (its surface parts 1a) is subjected to heat treatment, which according to Figure 2 can take place in a chamber or oven 4. Temperatures (e.g. 600°C) and times for treatment in saturated water vapour can be chosen according to the said publication. The object of the heat treatment is to completely or partially crystallize the coating added in the chamber 2, which can be chosen with a thickness of the order mentioned above, preferably in the range of 0.1  $\mu\text{m}$  to 10  $\mu\text{m}$ .

In the present example, the degree of crystallization is estimated in percentages, with a degree of crystallization of 0% relating to an X-ray-amorphous surface whose thickness is at most about 50 nm.

After the treatment in the oven 4 has been carried out, the unit 1 is transferred to a station 5 according to Figure 3. The station comprises a container 6 with TS 7, for example BMP, in which the unit or its surface parts is/are dipped for a time which is chosen as a function of TS type, release function, drying time and/or other parameter (examples of suitable times can be between 30 and 60 minutes). By means of the said immersion, TS is applied on top of the crystallized CaP layer and can at least partially be drawn by suction into the crystal structure. In alternative embodiments and methods of application, TS can be applied additionally or alternatively in other stages in the coating application. Thus, for example, it is possible for TS to be incorporated in the stages according to Figures 1 and/or 2, which has been symbolically indicated by broken line arrows P1 and P2. In another embodiment of the invention, the TS layer can be applied in another way, for example by dropping or painting it on and/or spraying it on.

The station 5 can also comprise equipment for further treatment of the implant 1. Thus, further TS substance can be applied in a subsidiary station 5' in order to achieve double TS layers on the surface of the

implant 1. This second method can be carried out by painting 7', dropping 7'' or spraying 7'''. The concentration of TS in the solution can be identical or different in the various applications. It can be applied by brush 6', nozzle 6'' or spray unit 6'''. The station according to Figure 3 can comprise a further subsidiary station 5'' where, by means of equipment 6''', release-retarding, visco-elastic material, for example hyaluronic acid 7'''' is applied, for example by means of painting or spraying, in one or more layers on the surface(s) of the implant 1. The station according to Figure 3 can comprise a further subsidiary station 5''', and so on, where further application of TS layers and/or release-retarding layers are applied in the same way as at subsidiary station 5''.

Figure 4 shows the finished unit 1. After treatment in the station according to Figure 3, the implant can thus be provided with various layers, which has been symbolized by 1 which has a single layer of TS, 1' which has a double layer of TS, 1'' which has double layers of TS and release-retarding layers, 1''' which has further layers, etc. Alternatively, the CaP and TS layers can be applied using a different station arrangement, and reference may be made here to the possibility of plasma-sprayable Cap including TS.

According to Figure 5, the unit can consist of a screw implant provided with thread or threads and intended to be screwed into a jaw bone 8 which has been provided with a hole 8a in which to screw the implant. The invention can also be used on other types of implants. After application in the bone, TS and CaP are released into the bone structure in accordance with the description below. This release has been symbolized by arrows 9 and 10. In the illustrative embodiment, the unit/implant is made of titanium, i.e. biocompatible material.

Figure 6 shows possible examples of release functions for TS and CaP. In the diagram, the horizontal axis represents the time h and the vertical

- 11 -

axis represents the quantity  $m$ , the curves thus representing the specified quantity per unit of time. The curve 11 illustrates a desired release function from implants with multi-layers of TS and release-retarding agent as above. The layers in question can be intended to be released at the time  $h''$ . Depending on the degree of crystallization in the CaP layer(s), the said layer or layers can assume bone growth stimulation or maintain bone growth. The curve 12 represents CaP layers with amorphous or low-crystalline character which continues release of bone stimulation function to the bone. The curve 13 represents a medium-high degree of crystallization, for example 25-75%. The curve 14 represents a high degree of crystallization, meaning 75-100%. At 100% crystallization, the layer functions as a support of preferably surface-bound TS. Initially high bone growth stimulation can be followed by long-term stimulation and maintenance of bone growth can thus be achieved. The breakdown or release functions are or can be related to the actual acid environment. It is desirable for the initial bone growth stimulation to be rapid so that the times for healing and prosthesis application can be reduced compared to previous times. However, the bone growth stimulation must not be too rapid since this causes collapse within the grown bone structure. The invention can solve this problem by making possible precise selection of the release times. The time  $h_1$  can be chosen, for example, to be 2-4 weeks. The long-term stimulation can be chosen to be months or years after the period of incorporation.

Figure 7 shows on a greatly enlarged scale a part 1c of the unit 1. The part 1c in question can be part of a thread whose surface 1d is to be coated with one or more CaP layers 15 and with TS layers 16 applied on top of the latter. It should be noted here that the invention also satisfies the requirements for great surface fineness on the surface 1d (cf. said publication).

Figure 8 shows, again on an enlarged scale, how the crystal structure 15' has to a certain extent drawn TS 16' in.

In Figure 9, a CaP layer is indicated by 17.  
5 The layer is applied on the metal in question, for example titanium 18, on a surface 18a which can be worked with a greater or lesser degree of fineness. The layer 17 can have a degree of crystallization of 0-100%. A first layer 19 of TS is applied to the outer  
10 surface 17a of the layer 17. This is followed by a second layer 20 of release-retarding agent, on which a second layer 21 of TS is applied. A third layer 22 of TS is in turn applied on the layer 21. The layer combination shown is only one example.

15 According to Figure 9a, the CaP layer according to Figure 9 can also be divided into two or more layers 17', 17'' which can be provided with identical or different degrees of crystallization. The layer 17'' supports a TS layer on its outside, etc.

20 Figures 10, 11 and 12 show the time-dependent breakdown of the various layers in bone or tissue. Breakdown components in the tissue or the bone are symbolized by arrows 24. The initial bone-growth stimulation is symbolized by arrows 25, which  
25 stimulation is thus initiated by means of the outer layer 21' of TS. The titanium or equivalent has been designated by 18''.

In Figure 11, the bone growth has started and is shown by 24a. In the stage according to Figure 11,  
30 the outer layers 21' and 20' according to Figure 10 have completely or partially disintegrated. In the stage according to Figure 12, the layers 19', 20'' and parts of the layer 17''' have also disintegrated and resulted in bone growth 24a'.

35 The said components thus begin the breakdown with the outermost layer, after which breakdown proceeds successively, layer by layer, until the CaP layer is exposed and subjected to the components.

In Figure 13, reference number 26 shows a CaP layer and reference number 27 shows the metal in the implant. The layer 26 can be provided with depressions 26a, 26b or other irregular surface structures which can accommodate TS layers 28, 29, 30 of different geometrical extents along the outer surface of the CaP layer, etc.

In Figures 14 and 15, two implants 1'''' and 1'''''' with different initial layer structures have initiated bone growths 31 and 32, 33, 34, 35, 36, respectively. The first bone growth 31 has a sock-shaped appearance, while the second one is more O-shaped. A characteristic feature is that the bone growth function achieves very good osteoconduction around or osteointegration within the implant or implant parts, which guarantees good incorporation in the bone structure.

The invention is not limited to the embodiment given above by way of example, and can be modified within the scope of the attached patent claims and the inventive concept.

## PATENT CLAIMS

1. Implant (1) for application in bone (8), for  
5 example dentine, primarily of the human body, and  
comprising a unit which can be applied in the bone in  
question and which is made of biocompatible material,  
preferably titanium, characterized in that, at least on  
its surface parts cooperating with the bone, it is  
10 provided with a coating (or coatings) comprising  
calcium phosphate compound(s), here called CaP, and a  
bone-growth-stimulating substance (protein), here  
called TS.
2. Implant according to Patent Claim 1,  
15 characterized in that the release time (h) for the said  
agents in the said coating (or coatings) for the bone  
or tissue concerned is chosen by setting the release  
time for CaP and the release time for TS in relation to  
each other.
- 20 3. Implant according to Patent Claim 2,  
characterized in that the release time for CaP is  
chosen with the aid of the degree of crystallization in  
CaP, a higher degree of crystallization giving a longer  
release time, and vice versa.
- 25 4. Implant according to Patent Claim 3,  
characterized in that the degree of crystallization in  
CaP is chosen to give a total release time of at least  
2-4 weeks up to several months.
5. Implant according to any of the preceding  
30 patent claims, characterized in that the growth-  
stimulating substance TS is applied on the CaP  
structure.
6. Implant according to any of the preceding  
patent claims, characterized in that the CaP coating  
35 has a thickness in the range of between a few angstroms  
and 10  $\mu\text{m}$ , preferably between 0.1  $\mu\text{m}$  and 20  $\mu\text{m}$ , and in  
that each TS layer has a thickness of between a few  
angstroms and 1  $\mu\text{m}$ .

7. Implant according to any of the preceding patent claims, characterized in that all areas of the said parts are provided with a coating (or coatings).

8. Implant according to any of the preceding patent claims, characterized in that the coating (or coatings) consists (consist) of one or more layers (17, 17', 17'') of calcium phosphate compounds and one or more layers (19, 21, 22) of bone-growth-stimulating substance TS.

9. Implant according to any of the preceding patent claims, characterized in that the coating (or coatings) comprises (comprise) one or more layers (19, 21, 22) of TS and, if appropriate, CaP and release-retarding agents (20), for example hyaluronic acid.

10. Implant according to any of the preceding patent claims, characterized in that one or more layers of CaP (17, 17', 17'') have a high degree of crystallization which means that the layer or layers have the main purpose of functioning as supports for the layer(s) (19, 21, 22) of TS and, if appropriate, the release-retarding agent(s) (20, 20', 20'').

11. Implant (1) according to any of the preceding patent claims, characterized in that one or more layers (17, 17', 17'') of CaP have a low or medium-high degree of crystallization which means that the layer or layers have a support function for TS (19) and, if appropriate, layers (20) of release-retarding agent are included in the bone-growth-stimulating function.

12. Implant according to any of the preceding patent claims, characterized in that the layer or layers (17, 17', 17'') of CaP is/are located nearest to or on the actual surfaces (18a) of the implant, and in that one or more layers (19, 21, 22) of TS are in turn located on the CaP layer (17) or the outermost CaP layer (17'').

13. Implant according to any of the preceding patent claims, characterized in that in the case of two or more layers (19, 21) of TS, layer(s) or agent(s)



(20', 20'') with a release-retarding function for TS is/are interleaved with the TS layers.

14. Implant according to any of the preceding patent claims, characterized in that at least the layer  
5 (19) or the layers of TS with release-retarding agents (20) can be released with components (24) occurring naturally in the bone and/or tissue.

15. Implant according to Patent Claim 14, characterized in that the said layers and appropriate  
10 release-retarding agents are arranged or chosen to generate bone formation (31) in the surrounding tissue around the implant without the risk of excessively rapid bone build-up and bone fracture tendencies.

16. Implant according to any of the preceding  
15 patent claims, characterized in that the said layers and appropriate release-retarding agents are arranged to effect an initial optimal bone structure (24a') around the implant in combination with long-term bone growth or bone-growth-promoting function.

20 17. Implant according to any of the preceding patent claims, characterized in that one or more CaP layers (17, 17', 17'') contain hydroxyapatite or HA, and in that one or more layers (28, 29, 30) of the bone-growth-stimulating substance consist of a  
25 substance belonging to the superfamily TGF- $\beta$ .

18. Method for arranging, on an implant (1) for application in bone (8), primarily of the human body, and comprising a unit of biocompatible material (18), a coating (or coatings) with agent (substance) at least  
30 on those surface parts of the unit cooperating with the bone, characterized in that the said parts of the unit or the whole unit are/is coated with calcium phosphate compound(s), here called CaP, which is/are X-ray-amorphous or given a specific degree of crystallization  
35 in combination with bone-growth-stimulating substance (protein), here called TS.

19. Method according to Patent Claim 18, characterized in that CaP is first applied and crystallized completely or partially in one or more

layers (17, 17', 17'''), and in that TS is then applied in one or more layers (19, 21, 22), for example by means of the unit or parts being immersed in a bath of TS.

5 20. Method according to Patent Claim 19, characterized in that in the case of several TS layers (19, 21, 22), the first layer is obtained by immersing in or dropping on a TS solution (7) at a chosen concentration, in that the second layer is obtained,  
10 after drying of the first layer, by dropping on or painting on a TS solution (7') at the said chosen concentration or a second concentration which differs from the first concentration, and in that a possible third layer is obtained, after drying of the second  
15 layer, by dropping on or painting on a TS solution at the said chosen concentration or a third concentration which differs from the first and/or second concentration, etc.

21. Method according to Patent Claim 18, 19 or 20, characterized in that the release-retarding agent, for  
20 example hyaluronic acid (7'') or other visco-elastic substance, is applied, for example by painting, on the respective layer in question.

22. Method according to any of Patent Claims 18-21, characterized in that each CaP layer (17, 17', 17'') is  
25 applied by sputtering of CaP substance on originally essentially amorphous implant surfaces and by subsequent heat treatment.

23. Method according to Patent Claim 22, characterized in that on treating implant material  
30 comprising titanium, the application and the heat treatment of CaP (26) are carried out such that depressions (26a, 26b) are obtained in the CaP layer, which depressions contribute to increasing the  
35 attachment of the outer TS layer (28, 29, 30) in the CaP layer (26).

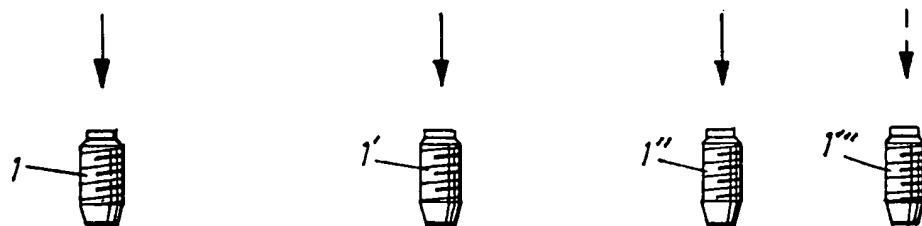
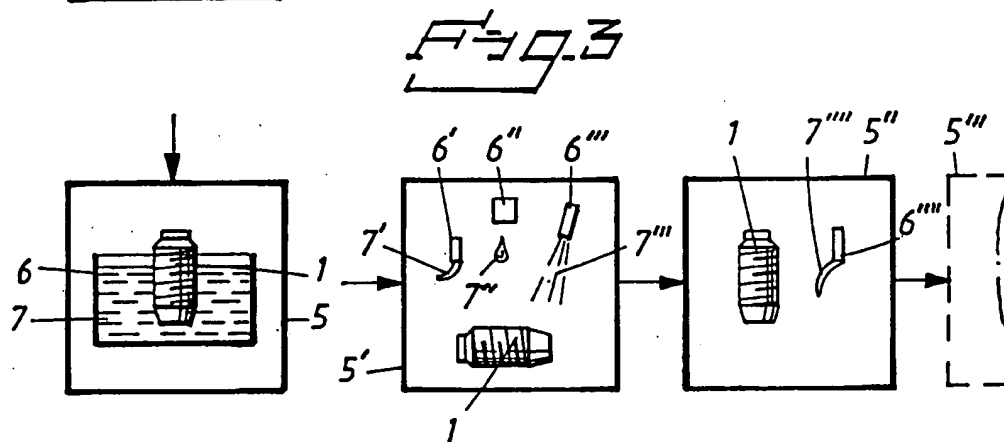
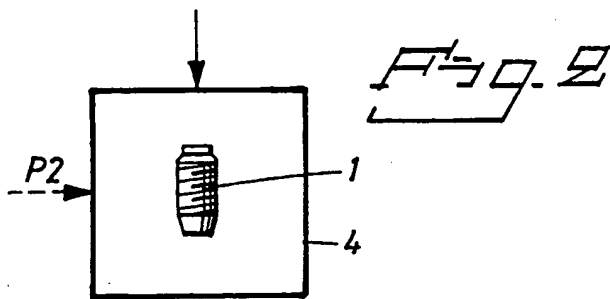
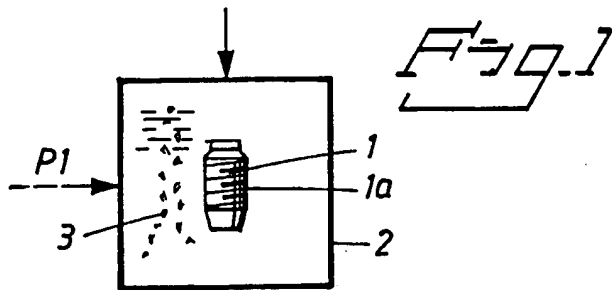
24. Method according to any of Patent Claims 18-23, characterized in that the implant is applied in a

threaded hole (8a) in the jaw bone (8) or equivalent bone.

25. Method according to any of Patent Claims 18-24, characterized in that the said layers are arranged for  
5 bone formation in different bone formation areas (32, 33, 34, 35, 36) seen from the implant's position in the bone, for example the jaw bone.

26. Use of an implant (1) for application in bone (8) and comprising a unit which can be applied in the  
10 bone and which is made of biocompatible material and, at least on its surface parts cooperating with the bone, is provided with a coating (or coatings), characterized in that calcium phosphate compound(s)  
is/are used together with bone-growth-stimulating  
15 substance (protein) in the said coating (or coatings).

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Fig. 5

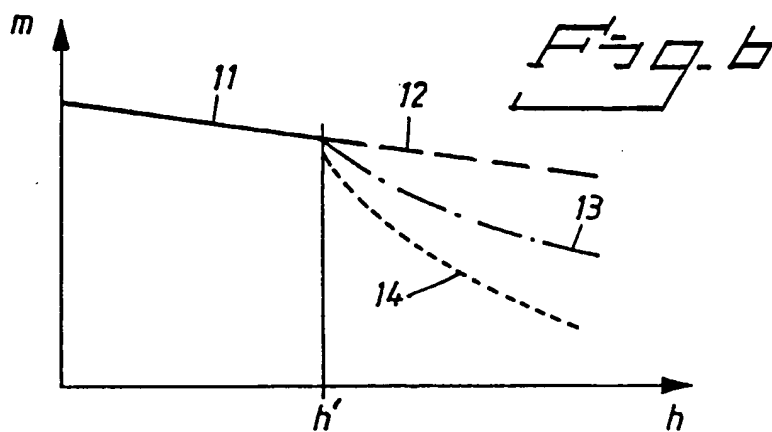
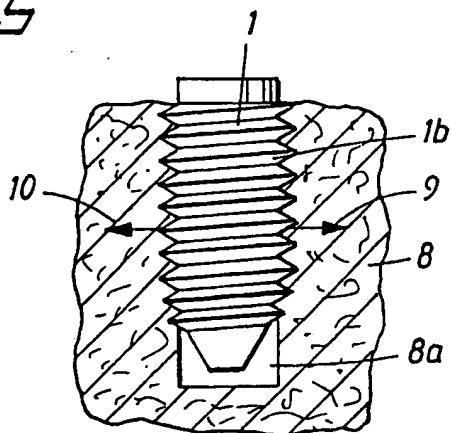


Fig. 7

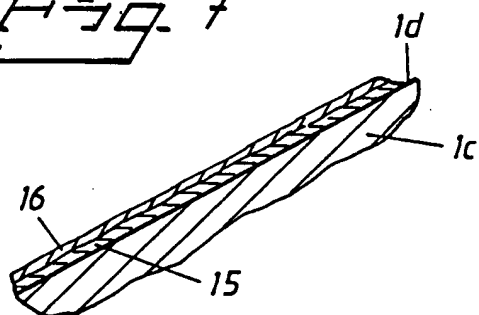


Fig. 8

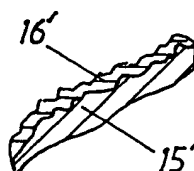


Fig. 9

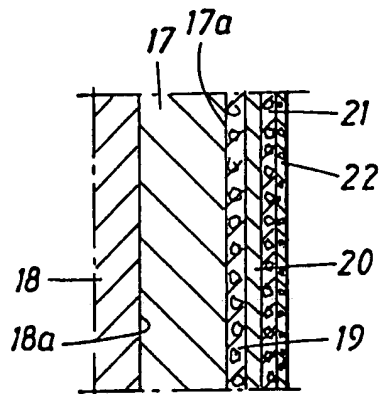


Fig. 9a

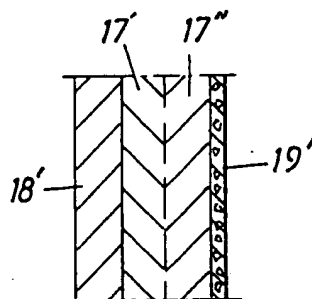


Fig. 10

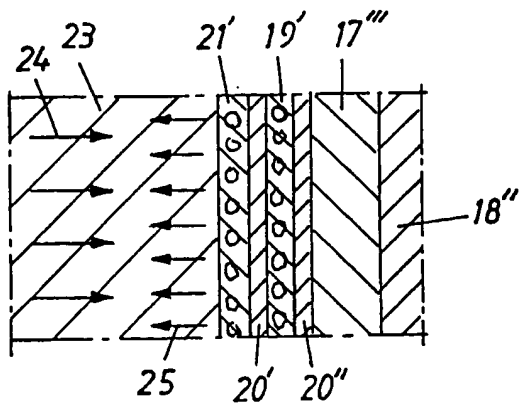


Fig. 11

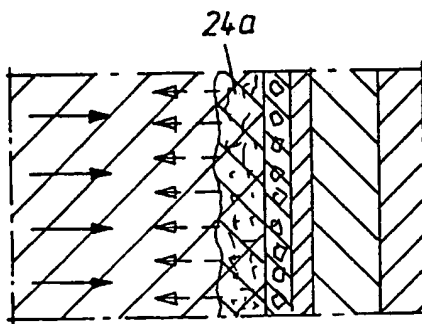
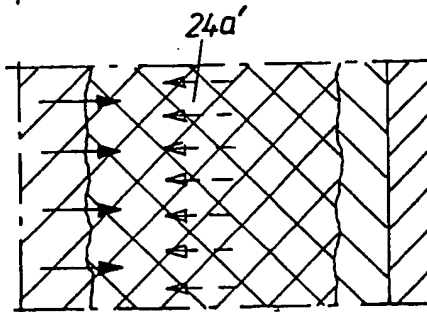


Fig. 12



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Fig. 13

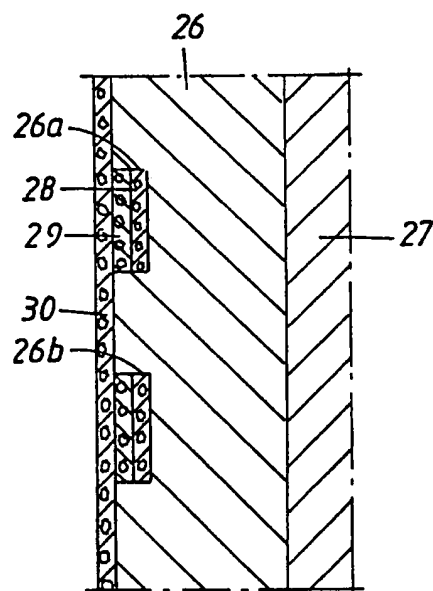


Fig. 14

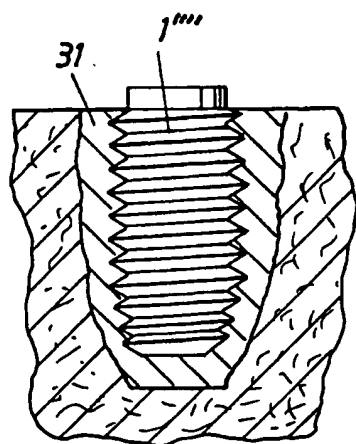
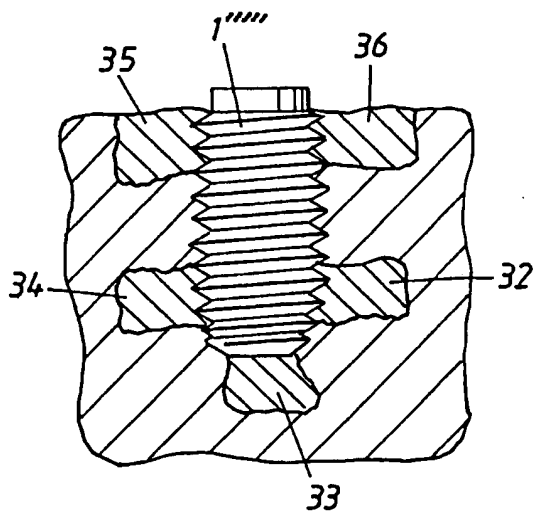


Fig. 15



## INTERNATIONAL SEARCH REPORT

International application No.

PCT/SE 00/01022

## A. CLASSIFICATION OF SUBJECT MATTER

IPC7: A61C 8/00, A61L 27/04, A61L 27/54

According to International Patent Classification (IPC) or to both national classification and IPC

## B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

IPC7: A61C, A61L

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

SE,DK,FI,NO classes as above

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

## C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	EP 0806212 A1 (MATRIX MEDICAL B.V.), 12 November 1997 (12.11.97), page 2, line 18 - page 3, line 14  --	1-23
A	US 4330891 A (PER I. BRANEMARK ET AL), 25 May 1982 (25.05.82)  --	1-23
A	WO 9848862 A1 (NOBEL BIO CARE AB), 5 November 1998 (05.11.98)  -----	1-23

☐ Further documents are listed in the continuation of Box C.
 ☒ See patent family annex.

## \* Special categories of cited documents:

- \* "A" document defining the general state of the art which is not considered to be of particular relevance
- \* "E" earlier document but published on or after the international filing date
- \* "L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)
- \* "O" document referring to an oral disclosure, use, exhibition or other means
- \* "P" document published prior to the international filing date but later than the priority date claimed

\* "T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

\* "X" document of particular relevance: the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

\* "Y" document of particular relevance: the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art

\* "&" document member of the same patent family

Date of the actual completion of the international search

18 Sept. 2000

Name and mailing address of the ISA/  
Swedish Patent Office  
Box 5055, S-102 42 STOCKHOLM  
Facsimile No. +46 8 666 02 86

Date of mailing of the international search report

20 -09- 2000

Authorized officer

Jack Hedlund/Els  
Telephone No. +46 8 782 25 00



## INTERNATIONAL SEARCH REPORT

International application No.  
**PCT/SE00/01022****Box I** Observations where certain claims were found unsearchable (Continuation of item 1 of first sheet)

This international search report has not been established in respect of certain claims under Article 17(2)(a) for the following reasons:

1. ☒ Claims Nos.: **24-26**  
because they relate to subject matter not required to be searched by this Authority, namely:  
**See PCT Rule 39.1(iv): Methods for treatment of the human or animal body by surgery or therapy, as well as diagnostic methods.**
2. ☐ Claims Nos.:  
because they relate to parts of the international application that do not comply with the prescribed requirements to such an extent that no meaningful international search can be carried out, specifically:
3. ☐ Claims Nos.:  
because they are dependent claims and are not drafted in accordance with the second and third sentences of Rule 6.4(a).:

**Box II** Observations where unity of invention is lacking (Continuation of item 2 of first sheet)

This International Searching Authority found multiple inventions in this international application, as follows:

1. ☐ As all required additional search fees were timely paid by the applicant, this international search report covers all searchable claims.
2. ☐ As all searchable claims could be searched without effort justifying an additional fee, this Authority did not invite payment of any additional fee.
3. ☐ As only some of the required additional search fees were timely paid by the applicant, this international search report covers only those claims for which fees were paid, specifically claims Nos.:
4. ☐ No required additional search fees were timely paid by the applicant. Consequently, this international search report is restricted to the invention first mentioned in the claims; it is covered by claims Nos.:

**Remark on Protest**

- ☐ The additional search fees were accompanied by the applicant's protest.  
☐ No protest accompanied the payment of additional search fees.

**INTERNATIONAL SEARCH REPORT**  
Information on patent family members

01/08/00

International application No.

PCT/SE 00/01022

Patent document cited in search report			Publication date	Patent family member(s)		Publication date
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				SE	9701647 D	00/00/00
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